Double functionalisation of carbon nanotubes for multimodal drug delivery†

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Multi-walled carbon nanotubes have been covalently functionalised via 1,3-dipolar cycloaddition of azomethine ylides with orthogonally protected amino functions that can be selectively deprotected and subsequently modified with drugs and fluorescent probes.

Functionalisation of carbon nanotubes (CNT) is a key step for the integration of this new material into different systems for technological and biomedical applications.1–8 One of the most powerful approaches for rendering carbon nanotubes soluble in a wide range of solvents is the covalent functionalisation of their side-walls and tips.9–11 As a consequence, functionalised carbon nanotubes (f-CNT) are emerging as novel components in nanovector formulations for the delivery of therapeutic molecules.5–8 f-CNT loaded with different peptides, proteins and nucleic acids are able to deliver their cargos into cells.12–20 Covalent functionalisation of CNT with drug (e.g. anticancer, antiviral or antibacterial agents) molecules is instead a field of research still poorly explored.21 The development of functionalised carbon nanotubes to target and be uptaken by specific cell populations without collateral consequences for healthy tissues would be of fundamental importance for example in cancer treatment.22,23 The molecular targeting of carbon nanotube delivery systems derivatised with a therapeutic agent is possible if an active recognition moiety is simultaneously present at the surface of the nanocarrier.23 In addition, attachment of a fluorescent molecule would provide optical signals for imaging and localisation of the CNT–drug conjugates. Therefore, multiple functionalisation of CNT is of particular interest for multimodal delivery of anticancer agents.

In this study we describe a straightforward methodology for the introduction of two orthogonally protected amino groups on the sidewalls of CNT, subsequently derivatised with fluorescein isothiocyanate (FITC) and methotrexate (MTX). MTX is a drug widely used against cancer, however, it suffers from low cellular uptake.24,25 Its conjugation to CNT represents a promising approach to overcome its limited cellular uptake by enhancing its internalisation via the f-CNT.15 For this purpose we exploited the 1,3-dipolar cycloaddition of azomethine ylides recently reported by our group.26–27 Diaminotriethylene glycol was initially mono-protected as tert-butyloxycarbonyl (Boc) as previously reported,27 or as benzylxycarbonyl (Z) (see ESI†). Both derivatives were subsequently reacted with benzyl- and tert-butyloxymethyl carbonate, respectively. Removal of the protection at the carboxylic functions via catalytic hydrogenolysis or acid treatment afforded the N-substituted glycines that were used for the 1,3-dipolar cycloaddition to multi-walled carbon nanotubes (MWNT) in the presence of paraformaldehyde at 130 °C in DMF (Scheme 1).

The reaction was conducted in the concomitant presence of an equimolar amount of both amino acids. After three days unreacted CNT were separated by centrifugation and f-MWNT were isolated by extraction with DCM (dichloromethane). Doubly f-MWNT were characterised by TEM and 1H NMR. In particular, the NMR analysis allowed observation of the resonances of the Z para-substituted glycines that were used for the 1,3-dipolar cycloaddition to multi-walled carbon nanotubes (MWNT) in the presence of paraformaldehyde at 130 °C in DMF (Scheme 1).

Scheme 1 (a) R-NHCH2COOH/(CH2O)n in DMF, 130 °C; (b) HCl 4 M in dioxane; (c) Ac2O; (d) TFA/TMSOTf/para-cresol. R = Boc-NH(CH2CH2O)2–CH2CH2– and Z-NH(CH2CH2O)2–CH2CH2–.

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cleaved first by treating MWNT 2 with HCl in dioxane. After liberation of the amino functions, we measured an amount of 0.35 mmol g⁻¹ of NH₂ (Table 1).

Before unmasking of the second protecting group, we blocked the free amines by direct acetylation (Scheme 1). Z group was then cleaved using a mixture of trifluoroacetic acid, trimethylsilyl trifluoromethanesulfonate and \( \text{para-cresol} \) (TFA/TMSOTf/\( \text{para-cresol} \)). Following precipitation and washings, we measured a loading of 0.35 mmol g⁻¹ of free amines (Table 1). This type of cleavage sequence is required by the Boc/Z protecting strategy, which implies two strong acid treatments for the removal of Boc and Z, respectively. This approach is somehow of limited application, since for further modifications following deprotection of Boc not all molecules are stable to the strong conditions used for Z cleavage. For this reason, a second strategy based on the complete orthogonality for the protection of the amino functions was explored. In this case, we prepared a mono-phthalimide (Pht) protected diaminotriethylene glycol, which was then reacted with benzylbromoacetate (see ESI†). The carboxylic function was liberated and the \( \text{N}-\text{glycine bearing the Pht} \) was mixed with an equivalent amount of the Boc-protected analogue and added simultaneously to the MWNT (Scheme 2).

MWNT 5 were observed by TEM (Fig. 1) and characterised again by \( \text{¹H NMR} \). Boc and Pht proton chemical shifts are present at around 1.40 and 7.00 ppm, respectively (see ESI†). The cleavage of Boc was performed using the acid conditions employed for MWNT 2, while Ph was removed using a solution of hydrazine in ethanol at room temperature under argon. The quantity of the free amino groups is reported in Table 1.

To prove the feasibility of double functionalisation of carbon nanotubes, we first removed Pht and labelled the tubes with fluorescein isothiocyanate (Scheme 2). Then, MWNT 6 were treated with HCl to eliminate the Boc group and coupled MTX.\(^{28} \)

MTX was activated at the carboxylic groups, using BOP [benzotriazol-1-yloxytris(dimethylamino)phosphonium hexafluorophosphate], and successfully coupled via the α or γ COOH to the free amino groups of Boc-deprotected MWNT 6. The negative Kaiser test confirmed the completeness of the reaction. The conjugate 7 was characterised using TEM (Fig. 1) and UV-Vis spectroscopy (see ESI†). TEM analysis of the conjugate 7 showed morphology very similar to MWNT 5.

We have subsequently evaluated the capacity of the bifunctional MWNT 7 to penetrate into the cells by epifluorescence and confocal microscopy. Human Jurkat T lymphocytes were cultured using RPMI 1640 medium at 37 °C. MWNT 7 were added to the cells at room temperature in a range of concentration between 0.05 and 5 \( \mu \text{g ml}^{-1} \), and the cells were incubated at 37 °C for 1 h. After this period, the cells were carefully rinsed, mounted on a microscope slide and observed under the microscope. Indeed, the presence of the fluorescence probe on the tubes has allowed the analysis of its internalisation and intracellular distribution.

### Table 1 Loading capacity of the doubly functionalised CNT

<table>
<thead>
<tr>
<th>Cleavage conditions</th>
<th>HCl/ dioxane</th>
<th>TFA/TMSOTf/( \text{para-cresol} )</th>
<th>Hydrazine/ EtOH</th>
</tr>
</thead>
<tbody>
<tr>
<td>Loading (mmol g⁻¹)</td>
<td>0.35 (3)</td>
<td>0.35 (4)</td>
<td>—</td>
</tr>
<tr>
<td>Loading (mmol g⁻¹)</td>
<td>0.30</td>
<td>0.65</td>
<td></td>
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\(^a\) Determined by the quantitative Kaiser test. \(^b\) The number in parentheses corresponds to the \( f\)-MWNT reported in Scheme 1. \(^c\) Amount of free amines for \( f\)-MWNT derived from 5 (Scheme 2) after Boc or Pht cleavage, respectively.

### Scheme 2

(a) \( \text{R–NHCH₂COOH/(CH₂O)}_{\text{n}} \) in DMF, 130 °C; (b) hydrazine in EtOH; (c) FITC in DMF; (d) HCl 4 M in dioxane; (e) MTX, Bop/DIEA in DMF. \( \text{R} = \text{Boc–NH(\( \text{CH₂CH₂O}_2\)-\( \text{CH}_{2}\text{CH}_2\text{–}) and Pht–N(\( \text{CH₂CH₂O}_2\)-\( \text{CH}_{2}\text{CH}_2\text{–})} \).
fast kinetics of uptake for the highest concentration of 5 \( \mu \text{g ml}^{-1} \) of MWNT 7.

Dose-response of the internalisation after incubation of Jurkat cells for 24 h at 37 °C with increasing amount of MWNT 7 [0.05 (thick grey line), 0.5 (thin black line) and 5 (thick black line) \( \mu \text{g ml}^{-1} \)]. FL1-H corresponds to FITC intensity.

Fig. 2A–C shows the epifluorescence and confocal microscopy images of the Jurkat cells after being treated with 5 \( \mu \text{g ml}^{-1} \) of MWNT 7. It is evident that MWNT 7 accumulates into the cytoplasm (Fig. 2B). The confocal analysis (Fig. 2C) clearly shows the presence of the labelled compound inside the cell localised around the nuclear membrane. We finally studied the dose and time dependence of the internalisation process. Fig. 2D shows the flow cytometry analysis of the cells treated with three different amounts of MWNT 7 for 24 hours. It is clear that the observed fluorescence signal is proportional to the dose. The rapid internalisation of the MTX by carbon nanotubes will be particularly advantageous for an improved efficiency of the drug action.

In conclusion, we have developed a novel strategy for the functionalisation of carbon nanotubes with two different molecules using the 1,3-dipolar cycloaddition of azomethine ylides. We have explored two alternative routes, which allowed introduction of a fluorescent probe and an anticancer agent around the CNT sidewalls. Controlled multifunctionalisation of CNT will certainly open new perspectives in the field of medical applications of f-CNT. For example, the attachment of molecules that will target specific receptors on tumour cells will help improve the response to anticancer agents. We are currently studying the cytotoxic activity of MTX conjugated to the fluorescent carbon nanotubes.

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Notes and references